# Linewidth-Resolved <sup>15</sup>N HSQC, a Simple 3D Method to Measure <sup>15</sup>N Relaxation Times from  $T_1$  and  $T_2$  Linewidths

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**A three-dimensional approach for measuring 15N relaxation times is described. Instead of selecting particular values for the relaxation period, in the proposed method the relaxation period is incremented periodically in order to create a 3D spectrum. This additional frequency domain of the transformed spectrum contains the relaxation time information in the**  $T_1$  and  $T_2$  **linewidths, and thus the longitudinal and transverse 15N relaxation times can be measured without determination of 2D cross peak volumes/intensities and subsequent curve fitting procedures.**  $\circ$  2001 Academic Press

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# **INTRODUCTION**

Continuous interest has been focused on measuring relaxation times,  $T_1$ ,  $T_2$ , and  $T_{1\rho}$ . These time constants provide information over the dynamic behavior of the molecule in question. In protein NMR, characterization of  ${}^{15}N$  and  ${}^{13}C$  relaxation times  $(T_1, T_2, \text{ and } T_{10})$  and heteronuclear NOE-values are commonly used in studying global protein motions as well as internal backbone mobility  $(1-6)$ . Further, the use of <sup>15</sup>N relaxation times in combination with residual dipolar coupling information ( ${}^{1}D_{NH}$ ) allows the identification of conformational exchange of protein backbone, as there is a structure dependence of  $^{15}N$  $T_1/T_2$  ratios and dipolar couplings in anisotropically tumbling proteins (*7*).

Although a wealth of relaxation data for protein could be collected if  $T_1$ ,  $T_2$ , and  $T_{1\rho}$  were measured for <sup>1</sup>H, <sup>13</sup>C, and <sup>15</sup>N, it is quite common routine to limit the relaxation measurements to <sup>15</sup>N, as this data combined with <sup>15</sup>N $\{$ <sup>1</sup>H $\}$ -NOE measurements usually provide enough information to determine the dynamic properties of a protein backbone. The <sup>15</sup>N  $T_1$ ,  $T_2$ , and  $T_{1\rho}$  values are usually measured by recording a set of 2D<sup>15</sup>N-HSQC spectra with different delays  $(T_r)$  during which the relaxation (longitudinal or transverse) causes decay of signal intensity. The volumes (or intensities) of cross peaks are then measured as a function of delay *T*r, and subsequent fitting of volumes (or intensities) to exponential function results in the relaxation time values (*1–4*). The main inconvenience of this method is the integration of the 2D cross peak volumes, a task that is quite prone

to errors. The volume integrations can be circumvented by employing the constant-time accordion experiment (*8–11*). In this method, the relaxation period  $T_r$  is covaried in concert with the  $t_1$ period, and thus the relaxation time domain, *T*r, is projected onto *t*<sup>1</sup> domain (*10, 11*). This accordion relaxation data is analyzed in the  $t_1$  domain using HSVD  $(12)$  and Levenberg–Marquardt algorithms (*13*) in order to obtain relaxation times.

We have tried to find a method enabling the collection of reliable relaxation data avoiding the necessity to (a) determine volumes or intensities of 2D cross peaks and (b) perform separate curve fitting procedure. An experiment that fullfills these conditions can be readily constructed by discarding the constant time evolution, as well as the accordion approach from pulse sequences described by Mandel *et al.* (*10*) and Carr *et al.* (*11*), but returning to the true 3D experiment instead, where the relaxation period  $T_r$  is independently incremented. Thus, the relaxation information is directly coded into the lineshape in the particular frequency domain. Now, in the resulting 3D spectrum two of the frequency domains form a convetional  $2D<sup>15</sup>N$  HSQC spectrum, and the third domain contains the lineshape. Although the current approach is a direct application of ideas presented previously, to the best of our knowledge this kind of 3D experiment has not been described in order to determine <sup>15</sup>N relaxation times for proteins. It allows a simple and robust measurement of relaxation times from "relaxation" linewidths, and can be easily adopted for other heteronuclei as well.

### **DESCRIPTION OF THE METHOD**

The 3D pulse sequences for the measurement of  $^{15}N T_1$  and *T*<sup>2</sup> are shown in Figs. 1A and 1B, respectively. The presented pulse sequences are essentially similar to the 2D versions presented by Kay *et al.* with suppression of the interference from the dipolar/CSA cross-correlation contribution (*14*). There are only a few differences including the incrementation of the  $T_r$ period to create the third frequency dimension, an additional string of <sup>15</sup>N 180 $\degree$  pulses in  $T_2$  measurement, and purge periods prior to incremented  $T_r$  domain in both sequences. These differences will be discussed later in the text. For larger proteins, the pulse sequences presented in Fig. 1 can be modified for





**FIG. 1.** The 3D experiments for the measurement of <sup>15</sup>N relaxation times  $T_1$  and  $T_2$ . Pulse sequence for (A)  $T_1$  measurement and (B)  $T_2$  measurement. Narrow (wide) bars correspond to 90◦ (180◦) hard rectangular pulses. Gradient pulses are represented by narrow white half-ellipses denoted by g0–g9. White half-ellipse on <sup>1</sup>H-channel represents a selective 90° sinc-pulse on water resonance. The <sup>1</sup>H and <sup>15</sup>N-carrier positions are 4.7 (water) and 113.0 (center of <sup>15</sup>N-spectral region). All the pulses have *x* phase unless otherwise indicated. Delays:  $\Delta_{NH} = 1/4^{1}J_{NH}$ ,  $t_1$  = incremented delay (<sup>15</sup>N shift evolution),  $t_{g1}$  = gradient duration plus recovery delay,  $\delta_1$  and  $\delta_2$  = basic <sup>15</sup>N during the acquisition was accomplished using the GARP-1 sequence (20). Incrementation of  $T_r$  period is achieved by incrementing the loop counter N by suitable integer  $N_{\text{(inc)}}$ . For  $T_2$  measurement, the loop counter L is decremented from maximum value to 0 in course of  $T_r$  incrementation. The aforementioned element ensures that the number of applied <sup>15</sup>N 180<sup>°</sup> pulses and thus the induced heat is constant throughout the experiment. The phase cycle employed for sequence A is  $\Phi_1 = x, -x, \Phi_2 = 16(y), 16(-y), \Phi_3 = 2(-y), 2(y), \Phi_4 = 4(x), 4(y), 4(-x), 4(-y), \Phi_5 = x$ , receiver = x, 2(-x), x, -x, 2(x), -x, x, 2(-x),  $x, -x, 2(x), -x, -x, 2(x), -x, x, 2(-x), x, -x, 2(x), -x, x, 2(-x), x$ . The phase cycle for sequence B is  $\Phi_1 = x, -x, \Phi_4 = 2(x), 2(y), 2(-x), 2(-y), \Phi_5 = 0$ *x*, receiver = *x*, 2(−*x*), *x*. In both experiments, the N- and P-type coherences are recorded separately by inverting the sign of gradient g6 and the phase  $\Phi_5$  in synchrony. Axial peak displacement was obtained via the States-TPPI method  $(21)$  by inverting the phase  $\Phi_1$  and receiver on every second increment.

better signal-to-noise ratio by simply replacing the sensitivity enhanced HSQC (*15*) with the TROSY sequence (*16–19*).

As neither chemical shift nor coupling evolution are active during the  $T_r$  period, the resulting time dependence of the magnetization can be presented by

$$
I(T_r) = I_0 \exp(-T_r/T_{1,2}),
$$
 [1]

where  $T_{1,2}$  is either longitudinal or transverse relaxation time, depending on the pulse sequence used.

After Fourier transformation, this exponentially decaying signal in the *T*<sup>r</sup> time domain results in Lorentzian lineshape in the frequency domain, with the linewidth (FWHH) determined by Eq. [2], and thus relaxation time can be coveniently determined:

FWHH =  $1/(\pi T_{1,2})$ . [2]

The actual incrementation of the *T*<sup>r</sup> period is accomplished by incrementing the loop counter N (Fig. 1), i.e., the number of repetitions of the basic  $T_r$  element, by a suitable number (integer). For example, we selected a spectral width of 10 Hz for the third frequency dimension (SW<sub>LW</sub>) in the  $T_1$  measurement of ubiquitin (Fig. 2). Because the delay  $\delta_1$  was set to 2.5 ms, the time increment of 100.0 ms corresponding the  $SW_{LW}$  can be achieved by incrementing the loop counter N by  $N_{(inc)} = 10$ . Since the basic  $T_r$ -element has finite length, the "available" spectral widths are limited to some degree, although there is the possibility of making small adjustments to the length of the basic  $T_r$  element by changing the interpulse delays  $\delta_1$  and  $\delta_2$  (14). The total length of the basic  $T_r$  element for the  $T_1$  measurement is  $4\delta_1$  and  $8\delta_2$  for the  $T_2$  measurement; i.e., <sup>1</sup>H and <sup>15</sup>N 180 $\degree$  pulses are fitted in delays  $\delta_1$  and  $\delta_2$ . As the relaxation time is directly extracted from the linewidth, the use of window functions prior to zero-filling and Fourier transform is prohibited. Due to this fact,  $T_r$ (max) must be



**FIG. 2.** 2D planes and 1D traces of 3D *T*<sup>1</sup> (Figs. A–D) and *T*<sup>2</sup> experiments (Figs. E–H) acquired from 1.0 mM uniformly 15N-labeled ubiquitin, 90/10%  $H_2O/D_2O$ , 30 $°C$  at 600 MHz. The 3D spectra were recorded using pulse sequences presented in Fig. 1: (A, E) 2D HSQC plane; (B, F) expansions of 2D planes for taken at <sup>15</sup>N-shift position marked by an arrow in A; (C, D, G, H) 1D traces taken along linewidth-axis in Figs. B and F (horizontal axis), position from where the traces are taken are marked with arrows. Traces C, G, D, and H are taken at the positions indicated by upper and lower arrow, respectively. The measured linewidth is marked in Figs. C, D, G, and H. The 3D *T*<sup>1</sup> and *T*<sup>2</sup> experiments were performed using a Varian Unity INOVA 600 spectrometer. Spectral widths were 8000 Hz (<sup>1</sup>H) and 2000 Hz (<sup>15</sup>N) for both experiments.  $T_1$  experiment and  $T_2$  experiment were acquired using spectral width of 10 Hz (N<sub>(inc)</sub> = 10) and 25 Hz  $(N_{\text{line}}) = 4$ ) for linewidth-domain (SW<sub>LW</sub>), respectively. The initial value for the loop counter L of the *T*<sub>2</sub> experiment was 224. The <sup>1</sup>H and <sup>15</sup>N carrier positions were 4.7 (water) and 113.0 ppm (center of the <sup>15</sup>N spectral region. The  $T_1$  experiment was acquired using 8 transients, 2048 (<sup>1</sup>H, complex points) × 100 (<sup>15</sup>N, complex points)  $\times$  18 (linewidth-domain, real points). The same number of transients and increments were used in the  $T_2$  experiment except only 8 increments (real points) in linewidth-domain were performed. A combination of squared cosine bell and gaussian apodization function was applied in  ${}^{1}$ H and  ${}^{15}$ N dimensions. Linear prediction was applied in both experiments to extend linewidth-domain by 18 and 16 real points in the  $T_1$  and  $T_2$  experiments, respectively. Matrices were zero filled to 2048 ( ${}^{1}H$ ) × 256 ( ${}^{15}N$ ) × 512 (linewidth-domain, real points) prior to Fourier transform. Pulses:  ${}^{1}H$  90° = 5.1 µs;  ${}^{15}N$  90° = 9.5 µs; water selective 90° pulse = 1.422 ms (one-lobe sinc at RF power of 175 Hz). Delays: relaxation delay = 2.5 s,  $\Delta_{\text{NH}}$  = 2.63 ms,  $t_{g1}$  = 0.350 ms,  $\delta_1$  = 2.5 ms, and  $\delta_2$  = 0.625 ms. Gradient strengths (durations):  $g0 = 16.0$  G/cm (0.5 ms),  $g1 = 11.2$  G/cm (0.5 ms)  $g2 = 16.0$  G/cm (0.5 ms),  $g3 = 22.0$  G/cm (1.0 ms),  $g4 = 16.0$  G/cm (1.0 ms),  $g5 = 36.0$  G/cm (1.25 ms),  $g6 = 26.0$  G/cm (2.5 ms),  $g7 = 4.0$  G/cm (0.5 ms),  $g8 = 6.0$  G/cm (0.5 ms),  $g9 = 26.0$  G/cm (0.25 ms). All the gradients were block shaped. <sup>15</sup>N-decoupling during the acquisition was achieved using GARP-1 (20).

relatively long in order to ensure sufficient decay of magnetization and thus the suppression of truncation artifacts. Fortunately, as the needed spectral width in the linewidth domain  $(SW_{LW})$  is usually small (and correspondinly the time increment is long), long enough  $T_r$ (max) can be reached with relatively few time increments. Furthermore, as only the decay of the signal intensity takes place during the  $T_r$  period, the data is purely real and thus one spectrum per 1/SWLW increment is sufficient. Additional reduction of the experimental time can be easily achieved by using linear prediction to calculate signal decay in the *T*<sup>r</sup> domain. This possibility is of particular importance when  $T_2$  values are to be measured. In  $T_2$  measurement using the linewidth method, relatively long  $T_r$ (max) of about 500–750 ms would be needed to ensure sufficient decay of magnetization in order to avoid truncation artifacts. Long  $T<sub>r</sub>$  periods (during which the modified CPMG pulse train is applied) may cause undue sample heating and may also eventually damage the probe. Therefore, in addition to obtained reduction of experimental time, it could be beneficial to use short  $T_r$ (max) and utilize linear prediction to extend the signal in the  $T_r$  domain. As mentioned above, compared to the sequence for  $T_2$  measurement described by Kay *et al.*, the pulse sequence presented in Fig. 1B contains an additional string of  $15N$  180 $\degree$  pulses (loop counter L). This element is incorporated in the sequence in order to minimize the possible effects of sample heating in the course of  $T_r$  incrementation (increasing number of  $15N$  180 $^{\circ}$  pulses). The loop counter L starts from maximum value of  $8 * N_{(inc)} * (ni(T_r) - 1)$ , where ni( $T_r$ ) is the number of increments in  $T_r$  domain and is decremented by  $8 * N_{(inc)}$ , whenever loop counter N is incremented. Another difference from the original pulse sequence is gradient purging period,  $90^{\circ}_{y}$ <sup>(15</sup>N)-*gradient*-90°<sub>-y</sub>(<sup>15</sup>N), prior to the modified CPMG pulse-train. The purpose of this purging period is to destroy all 15N magnetization that is not refocused during the preceding  $\Delta_{NH}$ -180°(<sup>1</sup>H), 180°(<sup>15</sup>N)- $\Delta_{NH}$ -period. Gradient purging is performed prior to the actual  $T_r$  element, as presented in Fig. 1A. All the  $15N$  magnetization that is not aligned along the *z* axis is destroyed by the gradient applied during the first  $\delta_1$ delay in propagator  $90^{\circ}_{\phi 2}({}^{15}\text{N})$ - $\delta_1$ -180° $({}^{1}\text{H})$ - $\delta_1$ .

# **RESULTS AND DISCUSSION**

The measurement of relaxation times  $T_1$  and  $T_2$  with 3D pulse sequences presented in Fig. 1 was demonstrated using 1 mM uniformly <sup>15</sup>N labeled ubiquitin (VLI Research) dissolved in 90/10% H2O/D2O, pH 4.7, 50 mM sodium phosphate buffer, at 30◦C. All the experiments were carried out using Varian Unity Inova 600 spectrometer equipped with a  ${}^{1}H/{}^{13}C/{}^{15}N$  triple resonance, actively shielded *z*-gradient probe. The relaxation times for selected 30 residues were extracted from linewidths in the dedicated frequency domain using Eq. [2]. The linewidths can be measured either manually (a method that is not completely objective), or by using a robust linewidth-determination method, which looks for maximum peak-top intensity and subsequently determines two data points representing the linewidth. In this work, we utilized the standard Varian Vnmr6.1d software macro for linewidth measurement (dres-command). Figure 2 presents the determination of  $T_1$  and  $T_2$  relaxation times for residues I13 and L67 using 2D expansions and 1D traces taken from the 3D spectra. Figures 2A–2D and 2E–2H correspond to 3D  $T_1$  and  $T_2$  experiments, respectively. Figures 2A and 2E show the  $2D<sup>15</sup>N$  HSQC planes of the 3D spectra. The cross peaks of residues I13 and L67 are located in the area marked with a box. Figures 2B and 2F show expansions of 2D planes of the 3D spectra taken at the positon in the  $15N$  axis marked with arrow. The cross peaks shown in these 2D planes contain the relaxation information coded into the linewidths. In order to measure the linewidths, the 1D traces were selected (traces are taken at the positions marked with arrows in Fig. 2B and corresponding 1D traces are shown in Figs. 2C, 2D, 2G, and 2H). In order to achieve as reliable relaxation times as possible, the 1D trace should be selected from the midpoint of the 2D contour (i.e., by selecting the maximum intensity 1D trace), although in theory, the linewidth in one dimension should be the same throughout the contour. In practice, deviations occur and are likely due to the S/N-ratio-drop induced errors in linewidth measurement when off-center 1D-traces are selected. In our case, the 1D traces were taken from the plane where the other axis was  ${}^{1}H$  (resolution 7.8 Hz/pt). The extraction of the 1D trace one point off from the center of the contour (maximum intensity 1D trace) resulted in an average error of about  $4\%$  in  $T_1$  values (10 residues were checked). The corresponding average error for the  $T_2$  values was 1%. Smaller errors in  $T_2$  values can be explained by the fact that the same amount of deviation in the linewidth measurement alters the  $T_2$  result less, as the linewidth corresponding to  $T_2$  is significantly larger. If better numerical resolution on the  ${}^{1}$ H axis was utilized, it could be assumed then that the misselection of 1D trace by one point in  ${}^{1}$ H-domain had a smaller effect on the results. In the case of peak-top overlap, one naturally must select a 1D trace from the region far from the overlapping contour center. In such cases, good numerical resolution could be useful in order to have continuous lineshape in the  ${}^{1}H$ -dimension (or  $15N$ , depending on which 2D plane is used to determine the linewidths). Good resolution of the other chemical shift axis (in our case 15N), in turn, would improve the accuracy of the 2Dplane selection. One factor, which also may affect the results, is phasing. Therefore, careful phase adjustments in all dimensions are recommended. The extracted 1D-traces were corrected for DC-offset. This ensured that macro (dres-command) used to measure linewidths performed correctly. It should be noted that extremely fine resolution in this linewidth-domain is crucial as relatively narrow linewidths must be measured accurately. The measured linewidths were converted into relaxation time data by using Eq. [2]. To compare the results obtained using the current approach, standard relaxation time analyses were performed for 3D data sets; i.e., the 2D  $^{15}N$  HSQC planes (corresponding to particular  $T_r$  value) were Fourier transformed and cross-peak volumes were measured as a function of  $T_r$ . The volume integration was performed using standard Vnmr6.1B software.



**FIG. 3.** Experimental <sup>15</sup>N  $T_2$  data of three residues I13, L67, and V70. The solid curves represent the best least square fits of the exponential function while the experimentally determined volumes are indicated with triangle, square, and circle for residues I13, L67, and V70, respectively. The presented experimental data is extracted from the 3D experiment as described in the text. The first experimental data point is recorded with *T*r-value 0.0 ms and subsequent points with steps of 40.0 ms, which corresponds to the selected  $SW_{LW} = 25$  Hz for the 3D  $T_2$  experiment. The last data point was recorded with  $T_r = 280.0$  ms.

Subsequent linear least-squares fitting of volumes to the exponential function (Eq. [1]) was used to extract the relaxation times. Figure  $\,$  3 presents volumes of 2D cross peaks from  $T_2$ measurement as a funtion of delay  $T_r$  and corresponding fitted exponential functions for three residues, I13, L67, and V70. Table 1 collects the  $T_1$  and  $T_2$  values measured with standard and linewidth techniques, and a corresponding graphical presentation is shown in Fig. 4. This plot, as well as Table 1, confirm that reliable values for relaxation times  $T_1$  and  $T_2$  can be obtained from linewidths using the proposed 3D pulse sequences. There are some visible differences between the two methods, but by percentage these are relatively small. These differences might be due to the somewhat limited numerical resolution in the linewidth domain (which causes an average uncertainty of 2.8% in linewidth determination for both  $T_1$  and  $T_2$  experiments). In addition to increasing the digital resolution, also fitting of Lorenzian lines could improve the accuracy of the current 3D methods. Particularly biased results are obtained for residue G76, which has relatively long  $T_1$  and  $T_2$  values compared to the relaxation times observed for other residues. Due to long relaxation times of G76, there is a significant amount of intensity left in the data point corresponding to  $T_r$ (max). Subsequent linear prediction (onefold for  $T_1$  measurement and twofold for  $T_2$  measurement for the presented relaxation data) was not sufficient to decay the signal intensity enough to avoid truncation artifacts in the linewidth domain. For other residues, no truncation artifacts were observed, and a good agreement of relaxation time results between classic and linewidth-based methods was obtained. Therefore, the current linewidth-based method must be interpreted with caution whenever severe truncation wiggles in the linewidth domain are observed. Fortunately, such residues can still provide reliable relaxation time information as the 3D data also permits the use of the classic volume/intesity measurement approach.

In order to perform a successful 3D linewidth-resolved experiment, a crude estimation of average relaxation times  $(T_1 \text{ or }$ *T*2) is needed. This enables the user to select sufficient spectral width,  $SW_{LW}$ , and the number of increments for the linewidthdomain to ensure the needed decay of the signal in the course of  $T_r$  incrementation. Notably, the average  $T_1$  and  $T_2$  values can be readily estimated from the decay of amide proton signals

## **TABLE 1**

Comparison of  $^{15}N$   $T_1$  and  $T_2$  Values for 30 Residues of  $^{15}N$ -**Labeled Ubiquitin Obtained Using Classic Curve-Fitting Procedures,** *T***1(Fit) and** *T***2(Fit), and 3D Linewidth Approach,** *T***1(3D) and** *T***2(3D)**

| Residue         | $T_1$ (Fit) [s] | $T_1(3D)$ [s] | $T_2$ (Fit) [s] | $T_2(3D)$ [s] |
|-----------------|-----------------|---------------|-----------------|---------------|
| Q2              | 0.449           | 0.451         | 0.176           | 0.172         |
| I3              | 0.435           | 0.444         | 0.181           | 0.164         |
| F <sub>4</sub>  | 0.422           | 0.416         | 0.177           | 0.179         |
| V <sub>5</sub>  | 0.444           | 0.450         | 0.186           | 0.188         |
| K <sub>6</sub>  | 0.433           | 0.436         | 0.174           | 0.178         |
| T7              | 0.432           | 0.434         | 0.176           | 0.174         |
| L8              | 0.392           | 0.418         | 0.189           | 0.178         |
| <b>I13</b>      | 0.438           | 0.433         | 0.174           | 0.177         |
| L15             | 0.436           | 0.438         | 0.172           | 0.174         |
| V17             | 0.428           | 0.429         | 0.176           | 0.173         |
| E18             | 0.456           | 0.471         | 0.178           | 0.179         |
| K27             | 0.420           | 0.403         | 0.172           | 0.168         |
| <b>I30</b>      | 0.434           | 0.417         | 0.185           | 0.178         |
| D32             | 0.439           | 0.420         | 0.186           | 0.181         |
| E34             | 0.458           | 0.442         | 0.187           | 0.182         |
| Q40             | 0.439           | 0.428         | 0.179           | 0.179         |
| L43             | 0.441           | 0.442         | 0.178           | 0.174         |
| <b>I44</b>      | 0.435           | 0.443         | 0.173           | 0.182         |
| F45             | 0.435           | 0.436         | 0.159           | 0.165         |
| L50             | 0.442           | 0.429         | 0.165           | 0.174         |
| D <sub>52</sub> | 0.491           | 0.481         | 0.187           | 0.178         |
| L <sub>56</sub> | 0.411           | 0.399         | 0.177           | 0.168         |
| N <sub>60</sub> | 0.438           | 0.419         | 0.181           | 0.173         |
| E64             | 0.427           | 0.426         | 0.176           | 0.175         |
| S65             | 0.425           | 0.420         | 0.173           | 0.171         |
| T <sub>66</sub> | 0.429           | 0.430         | 0.183           | 0.180         |
| L67             | 0.435           | 0.434         | 0.177           | 0.176         |
| H <sub>68</sub> | 0.442           | 0.439         | 0.183           | 0.185         |
| V70             | 0.430           | 0.415         | 0.161           | 0.163         |
| G76             | 1.220           | 1.159         | 0.797           | 0.389         |
|                 |                 |               |                 |               |

*Note.* Experimental parameters are described in the legend of Fig. 2.



**FIG. 4.** Graphical plot of data shown in Table 1. Relaxation times  $(^{15}N T_1)$ and  $T_2$ ) of residue G76 are omitted from the plot. Longitudinal <sup>15</sup>N relaxation times obtained using standard curve fitting and linewidth techniques are represented by cross and triangle, respectively, whereas the transverse <sup>15</sup>N relaxation times are represented by diamonds (fit) and circles (linewidth).

from a 1D relaxation series. In practice, selecting the number of increments so that  $T_r$ (max) is at least 1.0–2.0 times the average relaxation time, reliable relaxation data for most residues can be collected after performing one- or twofold extension of time domain using linear prediction. Of course, if the spectrometer time is not restricted, one can always use more increments in the linewidth-domain, especially for the  $T_1$ -measurement. For the *T*2-measurement, this is also possible if sample cooling-air of the spectrometer's temperature regulation unit can maintain the desired temperature and if the probe can tolerate a long string of <sup>15</sup>N 180 $\degree$  pulses. In our hands, the  $T_2$  results obtained using the linewidth method after data extension via twofold linear prediction were essentially similar to those obtained with standard *T*<sup>2</sup> measurement techniques, suggesting that one can use linear prediction procedures to extend data with predicted points at least twice the number of the original points.

In conclusion, the current 3D linewidth-based experiments allow the measurement of <sup>15</sup>N  $T_1$  and  $T_2$  relaxation times very conveniently from linewidths without separate volume/intensity measurement and fitting procedures. This should also hold for  $T_{10}$  measurements, as such an experiment can be readily constructed by modifying the pulse sequence presented in Fig. 1B. The time needed to perform these 3D experiments described is not much longer than performing a series of 2D experiments with selected  $T_r$  values. This arises from the fact mentioned earlier in the text that the data in the  $T_r$  domain is real and thus no imaginary part must be collected. In addition, further shortening of the needed experimental time can be readily achieved by extending the  $T_r$  domain with the aid of linear prediction. Furthermore, since the linewidths are used instead of 2D crosspeak volumes/intensities to determine 15N relaxation times, a good signal-to-noise ratio is not as crucial, as in the classic approach.

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## **REFERENCES**

- *1.* J. W. Peng and G. Wagner, *Methods Enzymol.* **239,** 563–596 (1994).
- *2.* L. E. Kay, D. A. Torchia, and A. Bax, *Biochemistry* **28,** 8972–8979 (1989).
- *3.* G. M. Clore, P. C. Driscoll, P. T. Wingfield, and A. M. Gronenborn, *Biochemistry* **29,** 7387–7401 (1990).
- *4.* J. W. Peng and G. Wagner, *J. Magn. Reson.* **98,** 308–332 (1992).
- *5.* P. Luginb¨uhl, K. V. Pervushin, H. Iwai, and K. W¨uthrich, *Biochemistry* **36,** 7305–7312 (1997).
- 6. S. F. Lienin, T. Bremi, B. Brutscher, R. Brüschweiler, and R. R. Ernst, *J. Am. Chem. Soc.* **120,** 9870–9879 (1998).
- *7.* E. de Alba and N. Tjandra, *J. Magn. Reson.* **144,** 367–371 (2000).
- *8.* G. Bodenhausen and R. R. Ernst, *J. Magn. Reson.* **45,** 367–373 (1981).
- *9.* L. E. Kay and J. H. Prestegard, *J. Magn. Reson.* **77,** 599–605 (1988).
- *10.* A. M. Mandel and A. G. Palmer III, *J. Magn. Reson. A* **110,** 62–72 (1994).
- *11.* P. A. Carr, D. A. Fearing, and A. G. Palmer III, *J. Magn. Reson.* **132,** 25–33 (1998).
- *12.* H. Barkhuijsen, R. de Beer, and D. van Ormondt, *J. Magn. Reson.* **73,** 553– 557 (1987).
- *13.* W. H. Press, B. P. Flannery, S. A. Teukolsky, and W. T. Vetterling, "Numerical Recipes: The Art of Scientific Computing," 2nd ed., Cambridge Univ. Press, Cambridge, UK (1986).
- *14.* L. E. Kay, L. K. Nicholson, F. Delaglio, A. Bax, and D. A. Torchia, *J. Magn. Reson.* **97,** 359–375 (1992).
- *15.* L. E. Kay, P. Keifer, and T. Saarinen, *J. Am. Chem. Soc.* **114,** 10,663–10,665 (1992).
- *16.* K. Pervushin, R. Riek, G. Wider, and K. W¨uthrich, *Proc. Natl. Acad. Sci. U.S.A.* **94,** 12,366–12,371 (1997).
- *17.* J. Weigelt, *J. Am. Chem. Soc.* **120,** 10,778–10,779 (1998).
- *18.* M. H. Lerche, A. Meissner, F. M. Poulsen, and O. W. Sørensen, *J. Magn. Reson.* **140,** 259–263 (1999).
- 19. T. Schulte-Herbrüggen and O. W. Sørensen, *J. Magn. Reson.* **144,** 123-128 (2000).
- *20.* A. J. Shaka, P. B. Barker, and R. Freeman, *J. Magn. Reson.* **64,** 547–552 (1985).
- *21.* D. Marion, M. Ikura, R. Tschudin, and A. Bax, *J. Magn. Reson.* **85,** 393–399 (1989).